AMENDMENTS TO THE SPECIFICATION

Please replace the paragraph beginning on Page 1, Line 3, and ending on Page 1, Line 5, with the following paragraph.

A1

This application is a [~~divisional~~] continuation of United States Application No. 09/774,869 filed on January 30, 2001, now U.S. Patent Number 6,537,314, entitled Percutaneous Mitral Annuloplasty and Cardiac Reinforcement.

Please replace the paragraph beginning on Page 19, Line 9, and ending on Page 19, Line 24, with the following paragraph.

A2

The overall length of the embodiment illustrated in Figure 5 should be sufficient that both of the first control line 108 and second control line 110 can extend outside of the patient, while the body 102 extends throughout the pathway of the ventricular girdle 100 as illustrated in Figure 6. For a percutaneous femoral vein access, the overall length of the device is therefore preferably at least about 200 cm, and generally within the range of from about 220 cm to about 260 cm. The length of the body 102 from proximal end 104 to distal end 106 is preferably sufficient to form a closed loop as illustrated in Figure 6. Although both heart size and the shape of the vascular pathway will vary from individual to individual, the length of the body 102 is generally within the range of from about 6 cm to about 12 cm. The body 102 may be injection molded, extruded as a tube, or coextruded over the wire which forms first and second control lines 108 and 110. Preferably, the body 102 either comprises or is coated with a material which is sufficiently compliant to minimize trauma to the vascular intima. Also, the transverse width of a tissue contacting surface [~~114~~] 115 on body 102 is preferably sufficient to distribute compressive force to minimize the risks of localized pressure necrosis within the coronary veins.

Please replace the paragraph beginning on Page 20, Line 9, and ending on Page 20, Line 19, with the following paragraph.

A3

Figures 11A-B show the proximal aspects of device assembly 200, and in particular various details for delivery assembly 210 that includes an outer member 215 that is generally tubular with an inner lumen 216 that is sized to house an inner member 225. Inner member 225 in the variation shown is generally tubular and is substantially free to rotate within lumen 216 by providing rotational force to inner member 225 proximally outside of the patient's body. According to the example shown, this rotational force is applied to inner member 225 via a thumbwheel 205 that is provided on proximal hub assembly 201 that is coupled to proximal end

portion 211 of delivery assembly 210. Thumbwheel 205 is rotationally coupled to inner member [~~25~~] 225 within hub assembly 201, which rotational coupling may be achieved according to a number of adaptions as would be apparent to one of ordinary skill.

Please replace the paragraph beginning on Page 21, Line 11, and ending on Page 21, Line 26, with the following paragraph.

According to one aspect of the rotational coupling, the prosthesis 250 is preferably held to resist rotation while rotational coupler 280 is rotated within the prosthesis 250. This may be achieved simply by frictional forces of surrounding tissue as prosthesis 250 is delivered into the desired vessel such as the coronary sinus. According to another example, this may be achieved by providing a releasable interface 218 such as a friction fit between outer member 215 and proximal end portion 252 of prosthesis 250, wherein the frictional engagement of outer member 215 and prosthesis 250 are held in a relatively fixed position while inner member 225 and rotational coupler 280 are rotated. This embodiment is shown in Figure 11A. In addition or in the alternative to the friction fit interface, a keyed interface may be employed as shown in Figures 12A-B. According to this mode, a shaped proximal fitting 253 on the proximal end 252 of prosthesis 250 is adapted to mate as a male counterpart into a shaped aperture or fitting on the distal end 212 of outer member 215. This keyed interface allows for rotational coupling between the members in a similar manner as just described for the inner member 225 and rotational coupler 280, and may allow for a more releasable coupling with reduced friction upon axial detachment of the members.